PRIMARY REPLACEMENT OF THE FRACTURED RADIAL HEAD WITH A METAL PROSTHESIS

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Compression testing of cadaver specimens showed that excision of the radial head allowed proximal radial displacement. The insertion of a metallic radial head restored normal mechanics, while a silicone rubber implant did not.

We reviewed 31 of 36 comminuted fractures of the radial head, 21 associated with dislocation or ulnar fracture, which had been treated by primary replacement with a Vitallium prosthesis. At a mean follow-up of 4.5 years, there was reliable restoration of stability and prevention of proximal radial migration. There had been no dislocations or prosthetic failures, but two implants had been removed for loosening. The prosthesis is recommended for use as a spacer to stabilise the elbow after severe injuries while the soft tissues heal.

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Replacement of the radial head has a controversial role in the acute management of comminuted fractures of the radial head. Excision of the head can give good long-term results (Morrey, Chao and Hui 1979; Goldberg, Peylan and Yosipovitch 1986; Coleman, Blair and Shurr 1987), but may be associated with persistent elbow or wrist pain, cubitus valgus, and proximal radial migration (McDougall and White 1957; Taylor and O’Connor 1964; Mikic and Vukadinovic 1983). Prosthetic replacement has been recommended to prevent these problems, improve stability, and allow early movement (Speed 1941; Cherry 1953; Swanson 1973).

Most reports of replacements of the radial head have included relatively few patients and only a short follow-up. Different materials have been used, but silicone rubber (Swanson, Jaeger and La Rochelle 1981) is probably the most popular, despite reports of fractures (Mayhall, Tiley and Paluska 1981; Morrey, Askew and Chao 1981) and sensitivity reactions (Gordon and Bullough 1982; Worsing, Engber and Lange 1982).

Amis et al (1979) showed that the radial head can transmit large forces, and Morrey et al (1981) found that replacement with silicone rubber had no objective functional advantage over simple excision. Carn et al (1986) demonstrated that silicone rubber compressed easily under physiological forces and transferred minimal load to the capitellum, possibly accounting for the progressive capitellar osteoporosis noted by Mackay, Fitzgerald and Miller (1979). Pribyl et al (1986) found that an acrylic implant resisted valgus angulation better than the softer silicone rubber. Harrington and Toutzas (1981) reported the successful use of a titanium implant in 15 patients, and recommended its use when stability was poor after excision of the radial head.

These reports suggest that there may be a role for a radial head prosthesis made of a stiffer material than silicone rubber; we describe the development and clinical trial of a Vitallium prosthesis (Howmedica (UK), London, UK).

MATERIALS AND METHODS

Implant development. Based on the measurement of 100 normal radiographs (Amis et al 1977) implants were designed in three diameters, with two thicknesses of radial head for each diameter. They were made for use without bone cement, having a pattern of grooves cast into the junction of the head and stem to allow the predominantly axial compressive loading to produce interlock (Fig. 1). The radius of the proximal rim of the head was larger than the anatomical radius to ensure that its edge would not dig into the capitellar cartilage.

The cleaned distal humerus and proximal radius of four fresh cadaver joints were mounted in a compression testing machine at 90° flexion (Fig. 2) using steel holders with bone cement. The radius was mounted below the
moving crosshead of the test machine with its head
centred on the load axis. The humeral tray was placed on
two pairs of rollers between flat plates; this allowed self-
centring of the radial head on the capitellum as load was
applied. The radius was loaded axially with up to 1 kN
force at a speed of 5 mm per minute, producing a load

versus displacement curve. This procedure was repeated
after replacement of the radial head by Vitallium and
then two sizes of silicone rubber implants (Silastic: Dow
Corning, Reading, UK), using this order because the
latter stems were larger. The resulting graphs (Fig. 3)
showed that metallic implants gave virtually normal
behaviour, whereas silicone rubber implants were de-
formed easily, allowing proximal radial migration under
load.

To study the contribution of the interosseous
membrane to the resistance of proximal radial migration,
two embalmed arms were tested, after the hand had been
removed at the radiocarpal joint and replaced by a steel
ball mounted distal to the radius by a cemented intramedullary stem. The radial head was removed
through a lateral incision and the soft tissues were
removed from the posterior aspect of the humerus which
was then mounted as in Figure 2. All other soft tissues
and the ulna were undisturbed. The interosseous mem-
brane was tested by loading the distal radius in a proximal
direction via the ball joint at 5 mm/min, so that secondary
movements were not prevented, and force versus deflec-
tion curves were recorded. Figure 3 shows that the
interosseous membrane gave intermediate bone displace-
ment behaviour, being stiffer than silicone rubber radial
heads and more compliant than natural and Vitallium
heads.

**Surgical technique.** The implants were inserted as soon as
possible, within 24 hours of the injury in all but two cases,
by a number of orthopaedic surgeons. Kocher’s lateral
approach was normally used, with Boyd’s posterolateral
approach when the olecranon had also been fractured.
Fragments of the radial head were removed and the
annular ligament was divided if necessary. The end of
the radial neck was preserved as far proximally as the
fracture allowed, since excessive bone removal would
have prevented load transmission through the implant.
The neck was reamed to an undersized stem cavity, and
the correct size of implant was chosen by trial articulation,
using radial head sizers without stems. The prosthesis
was then driven into position, uncemented, and the
annular ligament was sutured if this was possible.
Postoperatively, the elbow was mobilised within two
weeks.

**Clinical trial.** A total of 36 consecutive patients were
treated over a 6-year period, and 31 were reviewed: two
had died of unrelated causes and three were lost to follow-
up. Mean follow-up was 4.5 years (2 to 8), and there were
12 men and 19 women aged from 21 to 83 years (mean
57), at the time of follow-up. Each patient was reviewed
by two of the authors (DJK, LAR) and the results were
assessed clinically and radiologically.

Ten patients had an isolated comminuted fracture
of the radial head; in addition, eight had a fracture of the
olecranon (often extending into the proximal ulna) and
13 had elbow dislocation. Twenty-one patients had
sustained their injury in simple falls, nine had fallen from

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**Fig. 1**
The Vitallium radial head prosthesis, with an intramedullary stem and
a cast pattern of ribs and grooves at the junction between head and
stem. This is made in three diameters, with two head thicknesses for
each diameter.

**Fig. 2**
Diagram of a compression test for the radiohumeral joint. The
rollers beneath the humeral tray allow self-centring of the joint
under load.
RESULTS

Subjective assessment. At review, 24 of the 31 patients reported little or no elbow pain, six had some aching around the lateral side of the joint, but only with activity. One complained of pain at rest but no cause could be found.

Only two patients had wrist pain with normal activities, apart from an occasional ache. One of these had 10 mm subluxation of the distal radio-ulnar joint after removal of the prosthesis for loosening, and the other had normal wrist radiographs.

Objective assessment. Ranges of movement were compared with those of the normal limb, using a long-arm goniometer to measure flexion-extension and Patrick’s (1946) pendulum goniometer for pronation-supination.

The mean flexion deformity was 20° (0° to 55°). The mean loss of flexion was 10° (0° to 25°); the mean loss of pronation was 10° (0° to 30°) and of supination was 10° (0° to 60°). One elbow showed moderate valgus laxity, but the patient had no symptoms.

Complications. There were no cases of infection, prothropic fracture or dislocation. At review two patients had mild ulnar nerve paraesthesia. In two patients the prostheses had been removed for painful loosening; one of these also had a radio-ulnar synostosis which had been treated by the insertion of a silicone rubber sheet. Ten patients reported weakness compared with the normal side or had slightly reduced power on clinical testing by manual resistance to flexion and extension, comparing right and left arms. Grip strength was not assessed.

Radiography. Anteroposterior and lateral radiographs showed radiolucent lines around seven prostheses, but these did not appear to be progressive. We could make no reliable assessment of capitellar erosion or osteoporosis (Fig. 4).

Posteroanterior radiographs of both wrists were compared and revealed subluxation of the distal radio-
ulnar joint in two patients, in one by 2 mm and in the other by 10 mm. The patient with symptoms and 10 mm movement had had the prosthesis removed. Stress radiographs with the fingers clenched showed that muscle contraction did not affect these measurements.

DISCUSSION
There is no consensus about the treatment of an unstable elbow injury associated with fracture of the radial head. The options include early or delayed excision, reconstruction and replacement. Early excision of the radial head requires immobilisation for several weeks to allow the soft tissues to heal. There is a risk of redislocation and of stiffness. Reconstruction of the radial head is possible only when there are two or three main fragments: this may be technically difficult. Delayed excision of the radial head is sometimes performed several weeks later when necessary. Residual stability may be poor and there is a risk of myositis ossificans after delayed surgery.

For acute replacement of the radial head, the metallic prosthesis offers several advantages and avoids some of the disadvantages of silicone rubber. Its rigidity improves elbow stability when there has been gross soft-tissue tearing: we had no cases of redislocation. The internal fixation of an associated olecranon or proximal ulnar fracture may be poor because of comminution and osteoporotic bone: the use of a lateral spacer helps to share and balance the forces acting across the elbow, and allows earlier mobilisation. The Vitallium prosthesis was well tolerated, with a low incidence of symptomatic loosening and erosion. It did not break or cause inflammatory reactions.

We therefore recommend the use of this prosthesis as a spacer to aid stability while the bone and soft tissues heal. It can be removed at a later date if symptomatic loosening occurs, but it is usually well tolerated. In the longer term, this rigid implant should prevent proximal radial migration and the consequent valgus angulation of the elbow which has been reported to cause significant symptoms in two-thirds of previous reviews (McDougall and White 1957; Taylor and O'Connor 1964; Mikic and Vukanovich 1983).

Mechanical tests showed that for a given load, the radius migrated 2.6 times as far proximally after excision of the radial head than when intact, and that the Vitallium implant resisted this. After silicone rubber replacement, the radius still migrated 2.3 times as far as normal, and we believe that deflections would have been larger in fresh forearms, without the stiffening effect of embalming on the interosseous membrane. Figure 3 shows that the interosseous membrane still carried 86% of the load after replacement with silicone rubber. This explains why Morrey et al (1981) failed to find a functional advantage for silicone rubber replacement over excision alone.

Some of our patients had significant restriction of movement or pain on activity, but this correlated well with the severity of the initial injury. In our series 68% had dislocations or ulnar fractures or both; such severe injuries would have caused exclusion from those series which have reported generally good results for excision of the radial head.

Undisplaced radial head fractures are always treated conservatively; as the severity of the injury increases, the need for excision of the radial head increases and the controversial question of prosthetic replacement arises. We have not proved the case for the routine insertion of a prosthesis after resection for an isolated fracture of the radial head: similar results have been reported without the use of an implant. If the elbow is stable in flexion immediately after excision of the radial head, both our study and previous reports suggest that there is no advantage in replacement.

We emphasise that replacement must be carried out early, before soft-tissue contraction causes malalignment of the radial shaft on the capitellum. Late insertion was seen by the senior author (JHM) to cause malarticulation, impingement, and capitellar erosion.

Conclusions
1) Metallic radial head replacement restores the axial stiffness of the forearm to normal; excision and silicone rubber implants allow abnormal proximal migration under load.
2) A metallic prosthesis has a role in the acute management of severely displaced fractures of the radial head associated with dislocation or ulnar fracture.
3) Replacement of the radial head is not clearly better for an uncomplicated fracture; proof of this would require a prospective randomised trial.

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REFERENCES


